Article

Relationship Between Consonant Recognition in Noise and Hearing Threshold

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Purpose: Although poorer understanding of speech in noise by listeners who are hearing-impaired (HI) is known not to be directly related to audiometric hearing threshold, $HT(f)$, grouping HI listeners with $HT(f)$ is widely practiced. In this article, the relationship between consonant recognition and $HT(f)$ is considered over a range of signal-to-noise ratios (SNRs).

Method: Confusion matrices (CMs) from 25 HI ears were generated in response to 16 consonant-vowel syllables presented at 6 different SNRs. Individual differences scaling (INDSCAL) was applied to both feature-based matrices and CMs in order to evaluate the relationship between $HT(f)$ and consonant recognition among HI listeners.

Results: The results showed no predictive relationship between the percent error scores (Pe) and $HT(f)$ across SNRs. The multiple regression models showed that the $HT(f)$ accounted for 39% of the total variance of the slopes of the Pe. Feature-based INDSCAL analysis showed consistent grouping of listeners across SNRs, but not in terms of $HT(f)$. Systematic relationship between measures was also not defined by CM-based INDSCAL analysis across SNRs.

Conclusions: $HT(f)$ did not account for the majority of the variance (39%) in consonant recognition in noise when the complete body of the CM was considered.

Key Words: consonant confusions, audiometric hearing threshold, signal-to-noise ratio

P ure-tone audiometry is a well-established component of the audiometric test battery that measures behavioral hearing threshold to tones of different frequencies. For clinical and research purposes, many attempts have been made to test the correlation between speech recognition performance for hearing-impaired (HI) listeners and hearing thresholds. The results of such comparisons have generally shown little predictive value, particularly when speech recognition is measured in background noise (Festen & Plomp, 1983; Plomp, 1978; Smoorenburg, de Latt, & Plomp, 1982). Evidence of a poor predictive relationship between hearing threshold and sentence recognition performance in noise is well documented (Bentler & Duve, 2000; Killion, 2004a, 2004b; Lyregaard, 1982; Smoorenburg et al., 1982; Smoorenburg, 1992; Tschopp & Zust, 1994). The lack of

correlation between the measures may be related to differences in the simple acoustic signals used for pure-tone audiometry and the complex nature of speech recognition even though frequency-specific audibility deficits are known to affect speech perception (Bamford, Wilson, Atkinson, & Bench, 1981; Carhart & Porter, 1971). Perception of running discourse may take advantage of increased information from complex signals and contextual and linguistic properties of speech as well as the linguistic experience of the listener.

In contrast to using meaningful sentences, some studies have investigated the relationship between speech recognition and hearing threshold using nonsense syllables (Bilger & Wang, 1976; Danhauer & Lawarre, 1979; Dubno, Dirks, & Langhofer, 1982; Gordon-Salant, 1987; Reed, 1975; Walden & Montgomery, 1975; Walden, Montgomery, Prosek, & Schwartz, 1980; Wang, Reed, & Bilger, 1978). Using nonsense syllables is essential if investigators are interested in reducing the influence of contextual and linguistic factors so that recognition relies more on the use of acoustic features (Allen, 2005; Boothroyd & Nittrouer, 1988).

Previous studies have reported an inconsistent association between audiometric pure-tone thresholds and nonsense syllable recognition under different experimental methodologies. Four studies (Bilger & Wang,

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1976; Dubno et al., 1982; Reed, 1975; Wang et al., 1978) showed a systematic relationship associating better performance with lower thresholds, but another four studies (Danhauer & Lawarre, 1979; Gordon-Salant, 1987; Walden & Montgomery, 1975; Walden et al., 1980) supported no such relationship. A number of different approaches to analysis were applied across the studies.

In three studies that showed a systematic relationship with pure-tone threshold (Bilger & Wang, 1976; Reed, 1975; Wang et al., 1978), the relationship was evaluated with the results of a sequential information analysis (SINFA). SINFA provides the information for perceptual features embedded in confusion matrices (CMs) and determines the proportion of the information transmitted that is attributed to a given set of phonological features (Wang & Bilger, 1973). The procedure for constructing a (dis)similarity matrix for each subject can be summarized as follows. The results of a single SINFA were coded as a weighted vector for each of the stimulus features. The feature identified in the first iteration received the highest weight, the feature identified in the last iteration received the lowest weight, and the features not identified in the analysis received zero weight. Whenever the number of features identified exceeded the maximum weight, the lowest ranking features were all assigned weights of one. The similarity between any two subjects was defined as the sum of the products of corresponding feature weights. Finally the similarity matrices were submitted to Johnson's (1973) pairwise multidimensional scaling procedure to represent the similarities among subjects spatially. Using this SINFA-based approach, the three studies showed a systematic relationship between phoneme recognition and configuration of the pure-tone threshold, distinguishing listeners with normal thresholds, those with a flat hearing loss, and those with hearing loss with sloping audiometric configurations (Bilger & Wang, 1976; Reed, 1975; Wang et al., 1978).

Unlike the SINFA-based approach, a similarity judgment task was applied in another three studies in which no systematic relationship between performance and audiometric thresholds was reported (Danhauer & Lawarre, 1979; Walden & Montgomery, 1975; Walden et al., 1980). In the similarity judgment task the subject was asked to rate the similarity between a pair of syllables using equal interval scaling (i.e., 1 being *very similar,* 7 being *very dissimilar*). Similarity judgment allows the listener to consider perceptual qualities of the phonemes being compared in addition to recognition. For example, a HI listener can judge different speech sounds to be perceptually similar because they were correctly recognized as different phonemes but judged to be perceptually similar, or because they were incorrectly recognized and judged to be the same speech sound. The results of the similarity judgment were used as input for the individual difference scaling (INDSCAL)

model, a multidimensional scaling technique (Carrol & Chang, 1970). Using the similarity judgment the three studies showed no unique association between measures (Danhauer & Lawarre, 1979; Walden & Montgomery, 1975; Walden et al., 1980). It should be noted that even though Walden and Montgomery (1975) reported a systematic relationship between measures, the INDSCAL analysis with three-dimensional solutions revealed ambiguous subject space, particularly between sibilant and sonorant dimensions (see Walden & Montgomery, 1975, their Figure 2, p. 451).

Two studies analyzed phoneme recognition performance using raw CMs and compared the results with audiometric thresholds (Dubno et al., 1982; Gordon-Salant, 1987). Dubno et al. (1982) assessed consonant confusions at a fixed +20 dB signal-to-noise ratio (SNR; in cafeteria noise) in 38 HI listeners. A systematic relationship between consonant confusions and hearing threshold existed when the same consonant was given in error, most commonly for a given target across all three HI listener groups but with differences in error probability. That is, given a target /sa/, /θa/ was confused with the target at an error rate of 28.6% by the steeply sloping group, 10.4% by the gradually sloping group, and 4.2% by the flat group. However, the greatest percentage of errors was not consistently associated with a particular group. Moreover, the three HI groups were not completely separable when the complete CM was taken into account for acoustic feature (manner and place) analyses. Gordon-Salant (1987) measured CMs for consonant identification at +6 dB SNR (12 talkers babble) for three groups of elderly listeners (10 NH, 10 gradual sloping, and 10 steep sloping listeners). The INDSCAL analysis of these raw CMs revealed no unique relationship between consonant confusions and the audiometric characteristics.

In summary, the results of four studies (Bilger & Wang, 1976; Dubno et al., 1982; Reed, 1975; Wang et al., 1978) lead to the conclusion that consonant confusions are systematically related to audiometric hearing threshold. Another four studies (Danhauer & Lawarre, 1979; Gordon-Salant, 1987; Walden & Montgomery, 1975; Walden et al., 1980) support the opposite conclusion.

An important distinction between the studies discussed above is the use of different input structures to the INDSCAL model. If SINFA-based (dis)similarity matrices (Bilger & Wang, 1976; Reed, 1975; Wang et al., 1978) or partial raw CMs (Dubno et al., 1982) were used for the INDSCAL, a systematic relationship between syllable perception and pure-tone audiometric threshold was obtained. In contrast, when similarity judgment measures (Danhauer & Lawarre, 1979; Walden & Montgomery, 1975; Walden et al., 1980) or complete raw CMs (Gordon-Salant, 1987) were used as input to the INDSCAL, no systematic relationship was observed. Similarity judgment measures are directly used as input

for the INDSCAL. In contrast, SINFA-based measures should be carefully derived from raw CMs, and phonological features should be preselected by experimenters as input to the model. Consequently it is unclear how perceptual confusions embedded in CMs are reflected in SINFA-based (dis)similarity matrices. It is also unclear how the relationship between phoneme recognition and hearing threshold is impacted by these different input structures for the INDSCAL model.

Another issue in the previous studies is that CMs were measured in quiet (Bilger & Wang, 1976; Danhauer & Lawarre, 1979; Reed, 1975; Walden & Montgomery, 1975; Walden et al., 1980; Wang et al., 1978) or at +20 dB SNR (Dubno et al., 1982) and at +6 dB SNR (Gordon-Salant, 1987), which provided only partial information regarding the relationship between audiometric threshold and nonsense syllable recognition in noise. Finally, using nonsense syllables in noise provides the opportunity to evaluate performance with less use of contextual cues (e.g., meaning, grammar, prosody, etc.). These cues can increase speech understanding, particularly in noisy conditions, while not necessarily improving speech perception (Boothroyd & Nittrouer, 1988).

In the present study, we evaluate the relationship between audiometric threshold and nonsense syllable recognition with both SINFA- and CM-based INDSCAL

analyses over a range of SNRs. The data evaluated here were previously studied for a separate analysis (Phatak, Yoon, Gooler, & Allen, 2009) that provided a new method to quantify the degree of consonant perception loss relative to normal hearing listeners over a range of SNRs. During the analyses, we found that consonant confusions were not hearing-threshold specific, which led to motivation for this study. In the present study, we evaluated the relationship between audiometric thresholds and syllable recognition in noise in (a) mean performance-intensity functions, (b) correlation and multiple regression models having hearing threshold as predictors, and (c) SINFA-based and CM-based similarity matrices applied as inputs to the INDSCAL model.

Method
Participants

The 22 paid participants had sensorineural hearing loss, were native speakers of American English, and were between the ages of 18 and 64 years. Three listeners had bilateral hearing loss; hence each ear was tested separately (left and right ear identified as L and R), which resulted in a total of 25 ears tested. Descriptive information for listeners is given in Table 1.

Table 1. Descriptive information for listeners.

|	Sloping group			Flat group			Total across groups
	ID	Gender	Age	ID	Gender	Age	
	1L	F	21	3R	M	21	
	2L/R	F	59	4L/R	F	63	
	12L	F	39	76L	F	62	
	39L	M	63	113R	M	48	
	48R	M	62	177R	F	39	
	71L	M	60	216L	F	58	
	112R	F	54				
	134L	F	52				
	148L	M	60				
	170R	M	53				
	188R	M	64				
	195L	F	60				
	200L/R	F	52				
	208L	F	54				
	300L	M	54				
	301R	M	58				
Total # of listeners	16			6			22
Total # of ears	18			7			25

Note. Each listener is identified by ID number and ear tested (L: left or R: right). Three listeners whose performance was tested monaurally in both ears are indicated by ID plus L/R. Differences in number of listeners, ears, and audiograms vary because of the three listeners who were tested bilaterally. Listeners were divided into two groups on the basis of audiometric configuration: sloping group (18 ears) and flat group (7 ears).

Participants were recruited on the basis of screening preexisting audiograms obtained from the Department of Otolaryngology, Carle Clinic Association, Urbana, IL, and only those showing a three-frequency pure-tone average (0.5 kHz, 1 kHz, and 2 kHz) between 30 dB hearing level (HL) to 70 dB HL were recruited. Listeners whose hearing threshold was greater than 70 dB HL at $f \geq 2$ kHz were not enrolled in the study because of high mean error rates in preliminary testing (see the Procedure section). The pure-tone audiograms of all participants were also measured for this study and are shown in the upper panel of Figure 1. All procedures were approved by both the University of Illinois at Urban–Champaign Institutional Review Board and the Carle Medical Research Institutional Review Board.

Test Materials

Sixteen naturally spoken nonsense CV syllables composed of 16 American English consonants with the

Figure 1. *HT* (f) and the *Pe* (SNR) for the two audiogram-based groups. The upper panels are audiograms categorized by configuration of *HT* (f): sloping group (18 ears, left panel) and flat group (7 ears, right panel). The average *HT* (f) is indicated by a thick line. The lower panel shows the *Pe* (SNR) per listener. The mean *Pe* (SNR) for each group is shown by a thick line. For both top and bottom panels, data of two listeners having an audiogram with a slope of $\geq$ 30 dB/octave for 1 kHz $\leq$ f $\leq$ 4 kHz from the sloping group are indicated by thin-dotted lines. C_e is chance performance.
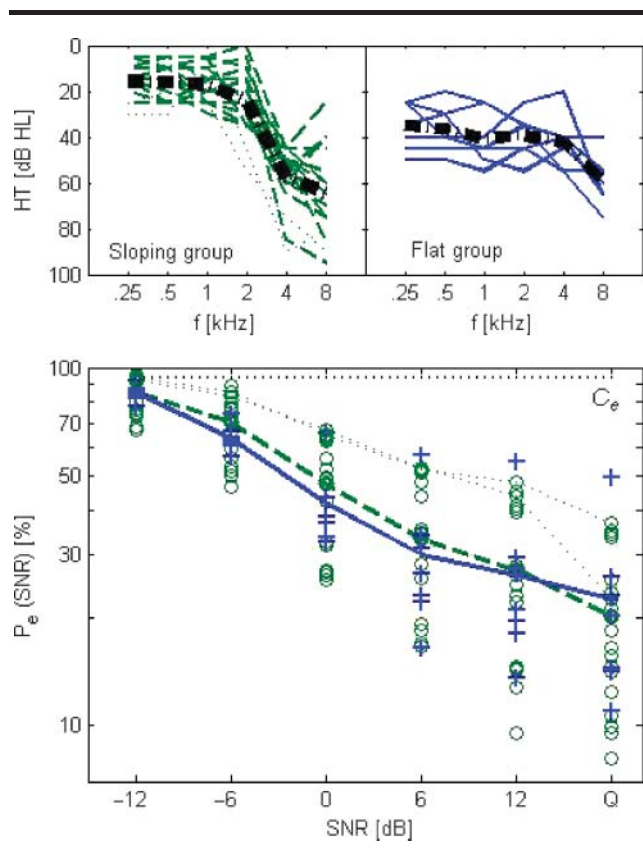
common vowel /a/ as in "father" were used as stimuli (Fousek, Svojanovsky, Grezl, & Hermansky, 2004). The 16 consonants presented were [/b/, /d/, /f/, /g/, /k/, /m/, /n/, /p/, /s/, /t/, /v/, /ð/, /ʃ/, /θ/, /ʒ/, /z/]. Half of these syllables were spoken by five talkers and the remaining syllables spoken by another five talkers, resulting in 80 tokens [(5 talkers × 8 CVs) + (5 talkers × 8 CVs)] in total. The purpose of dividing syllables among talkers was to create a diversity of talkers and simultaneously shorten experiment time. The use of multiple utterances from several talkers also offers some assurance about the generality of the analyses beyond the experimental stimuli.

The CVs were presented in speech-weighted noise with no spectral correction (gain) as a function of SNR (–12 dB, –6 dB, 0 dB, 6 dB, 12 dB, and in quiet [Q]). Each token was level-normalized before presentation using VU-meter software (Lobdell & Allen, 2007). No filtering was applied to the stimuli. The masker was a steady-state noise with an average speech-like power spectrum, identical to that used by Phatak and Allen (2007). For each CV, the RMS level of this noise was adjusted according to the level of the CVs to achieve the desired SNRs.

Stimuli were computer-controlled and delivered via an external USB audio card (Mobile-Pre, M-Audio), and presented monaurally via an Etymotic™ ER-2 insert earphone. Sound levels were controlled by an attenuator and headphone buffer (TDT system 3) so that stimuli were presented at the most comfortable listening level (MCL) for each listener. The MCL was determined by each listener's self-rating with the Cox loudness rating scale (Cox, 1995) in response to 30 CVs with no error in quiet. System calibration estimates that CV presentation levels in the ear canal were between 75 and 85 dB SPL.

Procedure

The ear canal was inspected otoscopically and pure-tone audiometry was performed to measure hearing thresholds and to confirm type of hearing loss for each listener. Each participant was seated in a sound-treated room (Industrial Acoustics Company) for audiometry, practice, and experimental sessions. Stimuli were presented to a test ear via an insert earphone. Environmental sound to the other ear was attenuated using a foam earplug.

CV syllables were presented while participants viewed the graphical user interface that listed the 16 CVs with example words alphabetically. Participants were asked to select the button on the interface to identify the perceived CV.

A calibrate button was included so that the presentation level (MCL) could be determined by a subject's response to playing 30 CV syllables in quiet. In addition,

pause and repeat buttons were available so that listeners could control the rate of stimulus presentation and could repeat the same stimulus without limit prior to responding. Our preliminary results with a few HI listeners showed no distinct influence of target repetition on performance.

Participants first performed a 30-min, two-practice-block (120 trials per block) session on CV identification in quiet with feedback. The eligibility to participate was determined by requiring the average percent error to be less than 50% across two practice blocks in quiet. If percent error score (Pe [SNR]) was ≥ 50% on the two practice blocks, two additional blocks were given to further consider eligibility for participation. Listeners became eligible to participate if Pe (SNR) was ≤ 50% on the second pair of practice blocks, but they remained ineligible if Pe (SNR) continued to be ≥ 50%.

We administered the consonant identification test to measure confusion matrices for CVs in speech-weighted noise as a function of SNR. For each presentation, a CV and SNR were selected and presentation randomized from the array of 16 CVs and six SNR indices (including Q). The set of individual stimuli [(8 CVs × 5 talkers) + (8 CVs × 5 talkers) × 6 SNRs = 480, named a set] was repeated six times (480 × 6 = 2880 trials in total), yielding 30 [2880 / (16 CV × 6 SNR)] repetitions of each CV at each SNR.

Each set (480 trials) was evenly distributed into four blocks (120 trials each), allowing participants to rest between blocks. No direct feedback about performance was provided for each CV presented. Percent correct feedback for each block was provided on the screen at the end of each block. The total number of trials and CVs already played were also provided on the screen.

Confusion matrices for each participant were plotted as a function of SNR. Any CV utterance produced by a particular talker that showed > 20% error in quiet for NH listeners was considered mispronounced and was removed from data analysis (Phatak & Allen, 2007). Total participation time to complete all protocols (pure-tone audiometry, CV practice, CV test, and break time) was about 6 hr and was performed in two visits.

Results
Audiometric Analysis and Pe (SNR)

The pure-tone audiograms were separated into one of two overall audiometric configurations to form a sloping group (*n* = 18; see Figure 1, top left panel) and flat group (*n* = 7; see Figure 1, top right panel). This classification was based on an historical scheme for describing the configuration of hearing threshold, *HT* (f), from the pure-tone audiogram (Bamford et al., 1981; Clark, 1981; Goodman, 1965; Margolis & Saly, 2007; Yoshioka &

Thornton, 1980). This classification scheme suggests that audiogram profiles can be classified by threshold configuration such as normal, flat, and sloping curves. In some studies the sloping curve is further divided into two subgroups, for example, sloping curves with a slope ≤ 20 dB/octave or ≥ 30 dB/octave for 1 kHz ≤ *f* ≤ 4 kHz (Clark, 1981; Goodman, 1965). Similarly, the flat curve could further be divided into two subgroups, flat curves with a slope ≤ 15 dB/octave or ≥ 25 dB/octave for 1 kHz ≤ *f* ≤ 4 kHz (Margolis & Saly, 2007; Yoshioka & Thornton, 1980). In our sloping group, only two out of 18 ears (denoted by the dotted line in Figure 1, top left panel) showed audiogram configurations with a slope ≥ 30 dB/octave for 1 kHz ≤ *f* ≤ 4 kHz; therefore, subgroups were not defined. However, any trends indicated by the data points for these two listeners will be noted. For the flat group, all seven listeners fell into a group having slopes ≤ 15 dB for 1 kHz ≤ *f* ≤ 4 kHz. The mean hearing thresholds (denoted as thick lines in the upper panels of Figure 1) differed significantly between the sloping and flat configuration groups, $F(1, 23) = 6.7$, $p < .05$. At frequencies < 2 kHz, *HT* (f) for listeners with sloping hearing loss was approximately 20 dB better than for listeners with flat configuration, whereas at frequencies > 3 kHz, *HT* (f) for the flat group is 15 dB better than for the sloping group.

A comparison of the *Pe* (SNR) between the two audiometric groups demonstrates a strong overlap in CV recognition performance with the range of *Pe* (SNR) exceeding 35% at each SNR. The lower panel of Figure 1 shows the *Pe* (SNR) across 16 CVs for individual listeners, coded according to the corresponding the *HT* (f). The mean *Pe* (SNR) for each group is shown by a thick line. A two-way repeated-measure analysis of variance showed no significant difference between the mean *Pe* (SNR) of the two groups, $F(1, 23) = 0.2$, $p > .05$. The main effect of SNR was significant, $F(5, 115) = 505$, $p < .001$. The error scores for the two listeners with slopes ≥ 30 dB/octave for 1 kHz ≤ *f* ≤ 4 kHz generally showed poorest performance among the listeners with sloping hearing loss.

In summary, we conclude that the audiogram-based listener grouping is poorly associated with the mean *Pe* (SNR) for nonsense CV recognition in noise. The results shown in Figure 1 indicate that the likelihood of demonstrating representative and distinctive descriptions of speech-recognition performance across a range of HI listeners would be low if built upon the audiogram-based listener grouping.

Regression Model

To better understand the contribution of frequency-dependent audibility to CV recognition, we investigated the extent to which thresholds of individual audiometric frequencies are associated with overall recognition

of nonsense CVs in noise. Specifically, we determined the extent to which listener's hearing thresholds account for the variance in Pe (SNR). To study this question, a multiple regression model was tested with the slopes of Pe (SNR) forming the dependent variable and with the HT (f) at standard audiometric frequencies, as the independent variable. These slopes were computed for each listener, based on a sigmoid fit without transformation.

The HT (f) at standard audiometric octave frequencies, namely, $x1$ through $x6$ for 0.25 kHz to 8 kHz, were used as predictors. The best model was determined by testing all combinations of the 6 predictors. The search for the best combination of the predictors was finalized by finding the smallest sum of least square errors and the highest adjusted R^2 values. As a result, HT (f) at 0.25 kHz, 2 kHz, and 4 kHz were included in the model as predictors. In the case of using multiple predictors, it is possible the predictors do not operate independently, but reveal multicollinearity, preventing an indication of the influence of individual predictors. Multicollinearity is > 0.1 for all six predictors, which indicates no violation of the assumption that predictors operated independently (Tabachnick & Fidell, 1989). Other important assumptions were addressed appropriately.[1]

The final linear regression model showed an insignificant relationship between the three predictors, HT (f) and the slopes of the Pe (SNR), $F(6, 18) = 1.93$, $p > .05$. This model explained 39% of the total variance, suggesting that the balance of the variance is associated with other unmeasured variables. Based on weights (β coefficients) for the model, the order of effects on the slope of Pe (SNR) from greatest to least is for thresholds at 2 kHz, 4 kHz, and 0.25 kHz.

INDSCAL Analysis

In this section, we attempt to use listeners' perceptual errors to identify the relationship between audiometric threshold and consonant confusions in noise. To display this relationship across subjects, we use the INDSCAL model (Carrol & Chang, 1970). The INDSCAL model takes each listener's (dis)similarity matrix (measured in a CM or similarity judgment) as its input, transforms each CM into Euclidean distances, and iterates a process of estimating individual subject differences by applying individual sets of weights to the dimensions of a common group space. In the subject space, each listener is represented as a point, and the

location of a listener in the subject space is adjusted by that subject's weights, indicating the particular salience to each of the dimensions of the space. In the present study, two-dimensional solutions were retained for both SINFA-based similarity matrices and raw CMs for each subject and for each SNR. A scree plot, a graph presenting a lack-of-fit INDSCAL model relative to dimensions, supports three-dimensional solutions as the optimal number of dimensions, but a squared correlation index, the proportion of variance of the optimally scaled data, with two-dimensional solutions is also acceptable (Takane, Young, & de Leeuw, 1977). Another reason for choosing two-dimensional solutions is to avoid the complexity of interpreting stimulus features across additional dimensions. The squared correlation index for the two-dimensional solutions revealed that the model accounts for a variance of 72% to 97% over the SNRs tested.

SINFA-Based INDSCAL Model

Subject space. Evaluation of subject weight in two-dimensional space, derived from the SINFA-based INDSCAL analysis, demonstrated no systematic relationship between stimulus features across SNRs and pure-tone threshold groups (see Figure 2). This result differs from that of Bilger and Wang (1976) despite obtaining (dis)similarity matrices using the same approach. However, two clear subject groups were identified, particularly by dimension (Dim.) 1. For example, seven subjects with flat hearing loss (ID is given) are consistently separated into two groups across SNRs except SNR = –12 dB; 3R and 117R were separated from other five subjects (4L, 4R, 76L, 113R, and 216L) by Dim. 1. The two listeners whose audiograms showed a slope $\geq$ 30 dB/octave for 1 kHz $\leq f \leq$ 4 kHz from the sloping group were also consistently classified in the same group across SNRs. This SINFA-based INDSCAL analysis revealed consistent groups of listeners across SNRs, but grouping was not consistent with the flat and sloping audiometric configurations.

To assess the consistency of these groups across SNRs, a retaining rate, the percentage of listeners remaining in the same group across SNRs, was computed, and the results are shown in top portion of Table 2. Overall retaining rate is constant across SNRs except –12 dB SNR. The retaining rates are given in each cell with the number of listeners in parentheses. Percentages oriented diagonally along the bottom of each column indicate the retaining rate between adjacent SNRs. For example, 23 listeners (92%) out of 25 maintained their groups between Q and 12 dB SNR and 16 (64%) out of 25 listeners were retained by their groups between –6 dB to –12 dB SNRs. Other cells indicate retaining rates for composite SNRs. For instance, 92% of listeners in the Q row remained in the same groups between

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[1]An assumption of normality of residual errors was tested by checking histograms for the residuals as well as normal probability plots. The linearity assumption between variables was verified by plotting bivariate scatter plots of the variables. In practice, these assumptions can never be fully confirmed; however in this case, linearity was read from these scatter plots.

Figure 2. Subject cluster, defined by SINFA-based INDSCAL analysis for each SNR. Subjects in the sloping group (*n* = 18) are represented by open circles;, subjects in the flat group (*n* = 7) are represented by their IDs. Two listeners with pure-tone average > 30 dB/octave are represented by thicker circles. Groups 1 and 2 were assigned in the quiet condition (lower right panel) for comparison with a study of Bilger and Wang (1976).
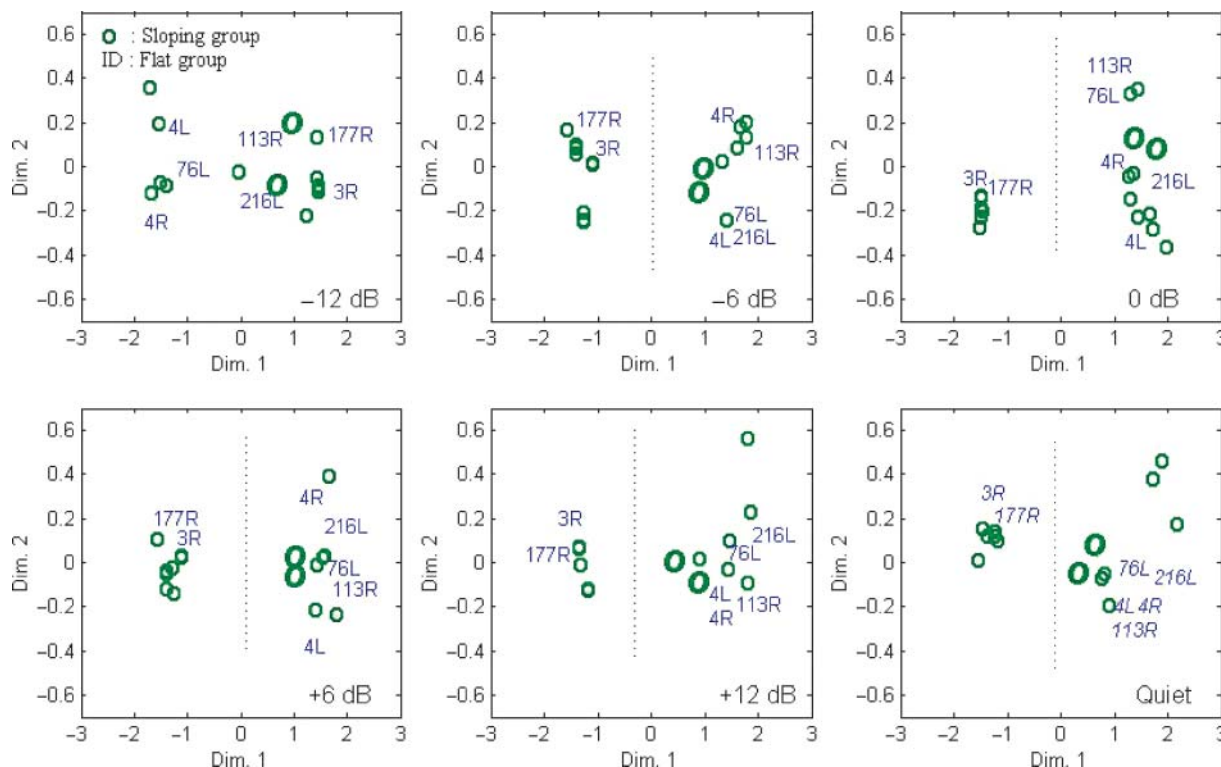
Q and 12 dB SNR, but the retaining rate decreased to 68% when groups were considered over 12 dB, 6 dB, –6 dB, and –12 dB SNRs. The retaining rate decreases considerably at –12 dB SNR.

Two of the three subjects whose performance was measured separately for the right and left ears (4L/R in the flat group; 200L/R in the sloping group) were consistently categorized in the same group across SNRs (results were shown only for 4L/R in Figures 2 and 4). The third subject who was tested bilaterally (2L/R in the sloping group) was categorized in the same group at –12 dB and 0 dB SNRs, but not at other SNRs.

Table 2. Retaining rate for SINFA-based (top) and CM-based (bottom) INDSCAL groups over SNRs.

INDSCAL group	SNR	12 dB	6 dB	0 dB	–6 dB	–12 dB
SINFA-based INDSCAL	Q	92% (23)	92% (23)	80% (20)	92% (23)	68% (17)
	12 dB		92% (23)	72% (18)	92% (23)	56% (14)
	6 dB			72% (18)	100% (25)	64% (16)
	0 dB				72% (18)	60% (15)
	–6 dB					64% (16)
CM-based INDSCAL	Q	52% (13)	40% (10)	40% (10)	24% (6)	8% (2)
	12 dB		68% (17)	60% (15)	36% (9)	12% (3)
	6 dB			76% (19)	44% (11)	12% (3)
	0 dB				60% (15)	20% (5)
	–6 dB					44% (11)

Note. The proportion of listeners who remained in the same group out of 25 listeners is given with the number of listeners in parenthesis. The set of diagonal cells formed along the bottom of each group specifies the retaining rate for adjacent signal-to-noise ratios (SNRs) and Q. SINFA = sequential information analysis; CM = confusion matrices; INDSCAL = individual difference scaling.

CM-based INDSCAL Model

Stimulus space. The group stimulus space illustrated in Figure 3 provides a graphical representation of the stimulus coordinates derived by CM-based INDSCAL. This group stimulus space depicts the perceptual proximities of the stimuli presumed to underlie all listeners' confusions. The dimensions are interpreted as the consonant features that can best account for the arrangement of the stimuli along each axis.

The stimuli appear to be arranged in two clusters along Dim. 1: the duration consonants (/s/, /ʃ/, /ʒ/, and /z/) are distinguished from the other 12 CVs at three lower SNRs (see Figure 3, top panels), whereas the fricative consonants (/f/, /s/, /v/, /ð/, /ʃ/, /ʒ/ and /z/) best define clusters at higher SNRs (see Figure 3, bottom panels). The feature labeled as duration is adapted from Miller and Nicely (1955) to distinguish four fricative consonants that are characterized by long duration and intense, high-frequency noise. The presence of a long frication noise appears to be the important feature for defining Dim. 1 at lower SNRs.

Dim. 2 shows that the nasals (/m/ and /n/) are separated from the other 14 CVs at the four higher SNRs (see Figure 3). A misplacement of /ʒ/ is observed for Dim. 2 at

+12 dB SNR. At –6 dB and –12 dB SNRs, the consonants on Dim. 2 are arranged in a single cluster, which precludes defining that dimension with an interpretable feature. For Dim. 2, the manner of articulation clearly serves as the common perceptual dimension at the four higher SNRs.

Subject space. The subject weights on two-dimensional solutions of the CM-based INDSCAL process with 25 HI ears are shown in Figure 4. A dimension weight reflects the strength of the dimensional property in accounting for the confusions made by each subject at each SNR. That is, the weights reflect the types of confusions made by subjects at each SNR. For example, if the confusions are mainly between stimuli that share stimulus features specified by a dimension, then subject weights will be relatively high for that dimension. Where the confusions are mainly between stimuli that do not share stimulus features described by the dimension, the subject weights for that dimension are relatively low.

The result of the CM-based INDSCAL analysis shows no discernible categorization of listeners between the two audiometric groups at any SNR, including the quiet condition (see Figure 4). At each SNR, listeners were grouped (A, B, and C), based on differences in

Figure 3. Group stimulus derived by the CM-based INDSCAL model at each SNR. Dimension 2 is not precisely determined at SNRs = –12 dB and –6 dB.
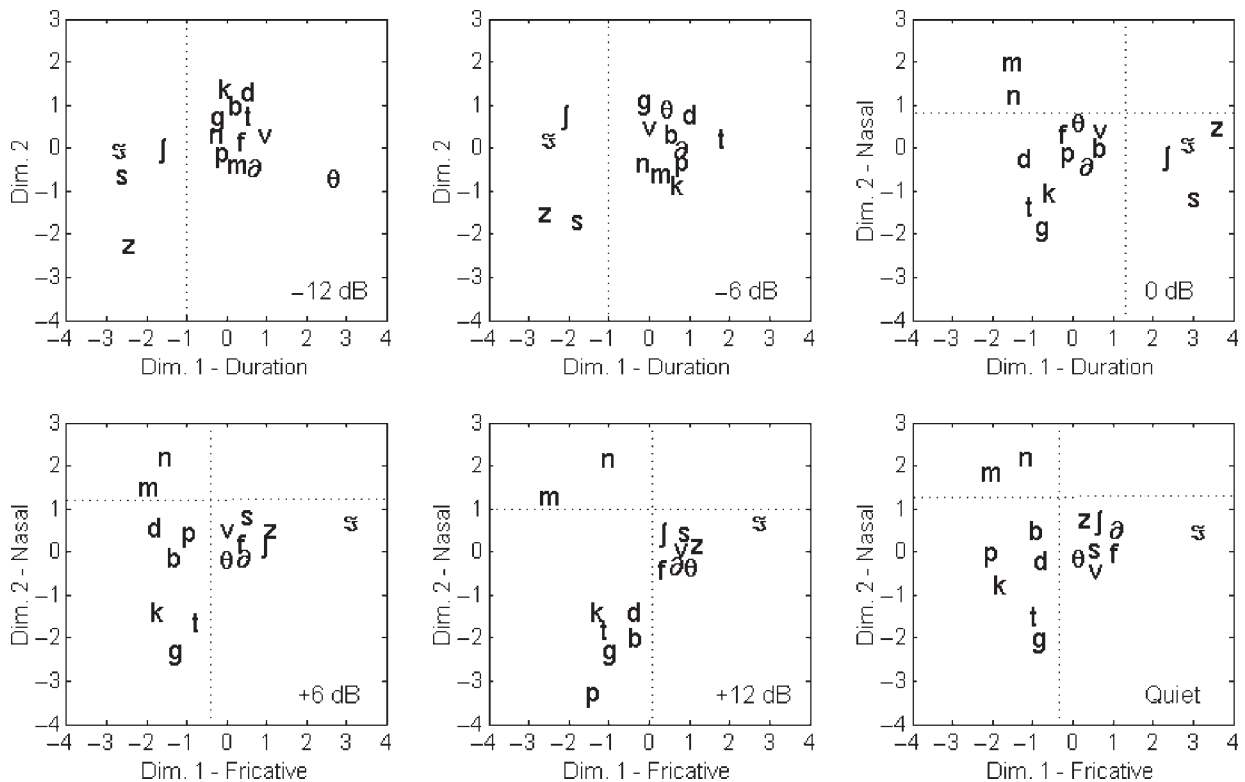
Figure 4. Listener distributions in subject distance space, assessed by the CM-based INDSCAL model at each SNR. Members of the sloping group are denoted with open circles; flat group members are denoted with their IDs. At each SNR, each data cluster is labeled as A, B, and C, although actual subjects within each cluster vary according to SNRs. Two sloping group listeners with slopes ≥ 30 dB/octave for 1 kHz ≤ f ≤ 4 kHz are denoted by thicker circles. For better visualization of grouping, the abscissa and the ordinate are scaled differently in each SNR panel, but ranges of both axis limits are constant across SNRs.
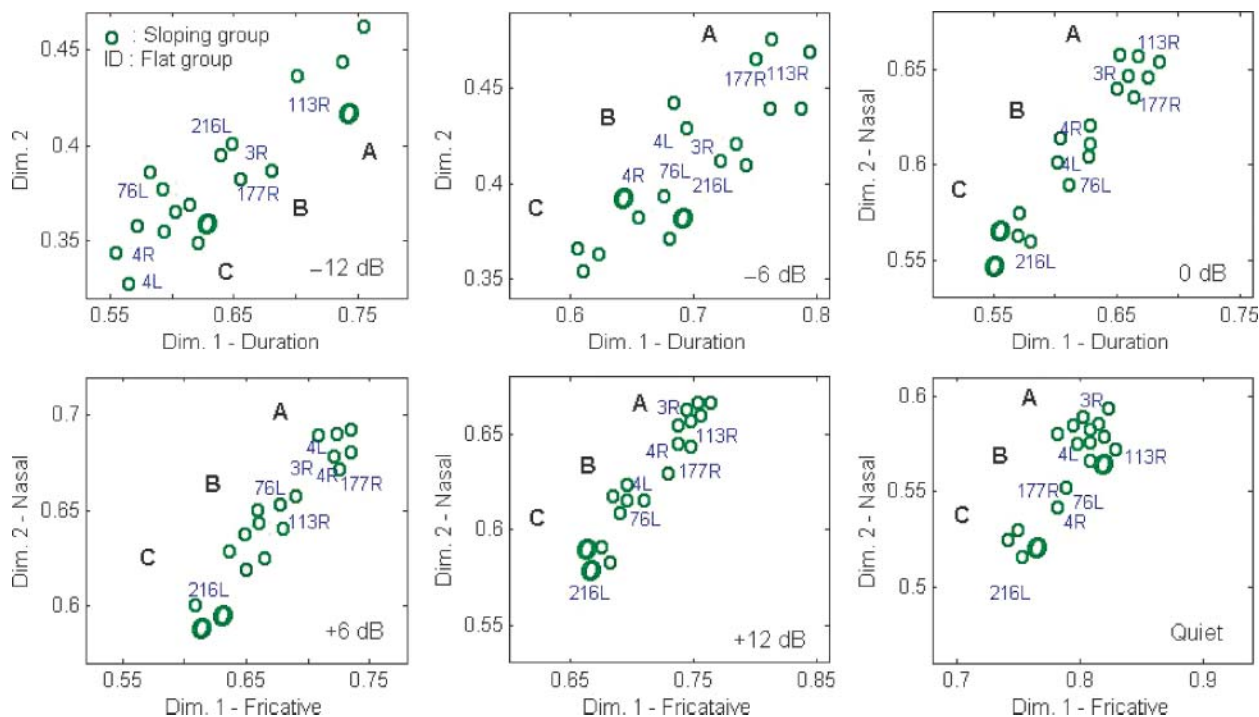
weighted Euclidean distances, although actual subjects within each cluster vary according to SNR. This CM-based group seems to be mainly dependent on the SNR, suggesting that confusions are a function of SNR, not of audiometric configurations. One noticeable pattern in the subject space is that listeners who had higher weights along Dim. 1 also had higher weights along Dim. 2. The variability of weights on both dimensions was noted for the two lowest SNRs. A distinct segregation of the two sloping group listeners with slopes ≥ 30 dB/octave for 1 kHz ≤ f ≤ 4 kHz is demonstrated, particularly at 0 dB, 6 dB, and 12 dB SNRs, but any unique separation from other sloping group listeners across SNRs is not obvious. Because no consistency in HI grouping was found, plots of audiograms versus CM-based groups are not presented. In addition, the subjects with both ears tested (4L/R in the flat group; 2L/R and 200L/R in the sloping group) were consistently categorized in the same group at the four lower SNRs, but not for the two higher SNRs.

The retaining rate for CM-based listener grouping is shown in the bottom portion of Table 2. The retaining rate is proportional to SNR, that is, as a SNR decreases, the retaining rate also decreases, particularly at a SNR < 0 dB. The rate is also largely poorer than that for the SINFA-based grouping. Out of 25 listeners, 13 (52%) maintained their groups between Q and 12 dB SNR and 11 (44%) were retained by their groups between –6 dB and –12 dB SNRs. Other cells indicate retaining rates for composite SNRs. For instance, 52% of listeners in Q row remained in the same groups between Q and 12 dB SNR, but the retaining rate decreased to 24% when groups were considered over 12 dB, 6 dB, and –6 dB SNRs. Finally only two listeners (8%) remained in the same groups over four SNRs from 12 dB to –12 dB. This retaining rate would vary with the SNR step size being compared. If equal step sizes are compared on the diagonals formed along the bottom of columns in Table 2, then a U-shaped function is more apparent with the best retention rate for comparisons at 0 dB SNR. Indeed, 0 dB SNR has the highest retention rate.

Discussion

The goal of the present study was to determine the extent to which audiometric hearing threshold is associated with nonsense CV recognition in noise. The

results revealed that the *Pe* (SNR) does not seem to be directly associated with the *HT* (f), as shown in Figure 1. However, in the quiet condition, the scores for the sloping hearing threshold group (20%) and for the flat hearing threshold group (25%) are similar to those reported by Dubno et al. (1982). Dubno et al. reported that errors among the listeners with sloping hearing loss were the lowest (22% error), whereas those with flat hearing loss were somewhat poorer (30% error), and those labeled steep hearing loss showed the highest error (50%) on CV or VC syllables in cafeteria noise at +20 dB SNR.

The multiple regression models revealed nonsignificant associations between the slopes of *Pe* (SNR) and *HT* (f). *HT* (f) contributed 39% of the total variances of the slope of *Pe* (SNR). The weights (β coefficients) for the model showed that effect on the slope of *Pe* (SNR) was the greatest for thresholds at 2 kHz. Carhart and Porter (1971) showed a similar finding for spondees: Adding a threshold at 1 kHz (except in the group with marked high-frequency loss) for the regression model was highly correlated with speech reception threshold (SRT), but adding threshold at 2 kHz to the model improved the prediction slightly. However, adding thresholds at 4 kHz and 0.25 kHz did not produce practical improvement in predictability for spondee SRT. Bamford et al. (1981) correlated pure-tone audiograms with the slope of sentence perception performance in quiet for 150 HI children. Poor correlation (*r* = 0.329) was reported. It was also reported that the correlation between measures was highly affected by the degree of hearing loss, particularly from severe to profound hearing loss.

SINFA-based listener grouping (see Figure 2) showed no unique relationship of audiometric characteristics with consonant confusions even though two distinct groups were consistently defined across SNRs. This poor relationship is related to two technical issues in the SINFA analysis.

First, the SINFA requires prior knowledge about unknown perceptual features embedded in CMs. In the SINFA procedure, phonological features are selected by the experimenter with some unknown assumption about the perceptual features. The analysis of SINFA-based INDSCAL provides only subject spaces without names of dimensions because experimenters select features for the model in advance. This is the reason that all studies that used SINFA never presented subject dimensions because the approach does not permit identification of that information. In addition, requirement of prior knowledge of perceptual features is a fundamental violation for INDSCAL model because the core concept of the INDSCAL model is to reveal unknown perceptual dimensions embedded in CMs or (dis)similarity matrices.

Another concern about using SINFA is related to the procedure for obtaining (dis)similarity matrices. As

discussed in the introduction, the feature identified in the first iteration received the highest weight, the feature identified in the last iteration received the lowest weight, and the features not identified in the analysis received zero weight. Whenever the number of features identified exceeded the maximum weight, the lowest ranking features were all assigned weights of one. The similarity between any two subjects was defined as the sum of the products of corresponding feature weights. This means that a similarity matrix for one subject might be much like that of another subject even though their features were identified in very different orders. For example subject A has ratings from 6 to 1 for the same set of features, but subject B has ratings from 1 to 6. The sum of the products between subjects A and B is 56. Another two subjects, C and D, have two top ratings (6 and 5) in common, but ratings for other features are not in common. The sum of the products between subjects C and D is 61. It is highly likely that the SINFA-based INDSCAL model would consider these two pairs of subjects similar even though their feature perception is completely different.

As shown in the two-dimensional subject space derived from the CM-based INDSCAL (see Figure 4), no unique relationship between audiometric thresholds and perceptual confusions was evident across SNRs, including the quiet condition. This CM-based INDSCAL grouping seems to be a function of SNR, not of audiometric configuration.

Our CM-based INDSCAL solutions for perception in quiet are consistent with results of other studies (Danhauer & Lawarre, 1979; Danhauer & Singh, 1975; Walden et al., 1980) despite differences in some experimental conditions including (in their studies): a single talker, listener's demographics, stimulus context (CV-CV pairs), and response mode (similarity judgment using 7-point equal-appearing interval scaling). Danhauer and Singh (1975) found that subject weights in the three-dimensional solutions generated by INDSCAL were neither obvious nor related to three different audiometric configurations. Danhauer and Lawarre (1979) also found that HI listeners represented in three-dimensional solutions could not be clustered into distinct subgroups according to three different configurations of hearing loss. Walden et al. (1980) also reported no consistent differences in feature weights between two HI listener groups represented by INDSCAL in four-dimensional solutions. This result is somewhat in disagreement with those of Walden and Montgomery (1975) who reported distinct HI listener groupings in three-dimensional subject space determined by the INDSCAL analysis. In contrast to a conclusion made by the authors, the INDSCAL analysis with three-dimensional solutions revealed ambiguous subject space, particularly between sibilant and sonorant dimensions

(see Walden & Montgomery, 1975, their Figure 2, p. 451). Compared with INDSCAL groupings from other studies, subject space in the study by Walden and Montgomery (1975) did not support distinct subject groups.

A study of CV perception in HI listeners by Bilger and Wang (1976) provides a particularly important comparison with the current study because the complete body of information from both diagonal and off-diagonal cells in CMs was fully taken into account for the analysis. Whereas 14 CVs used by Bilger and Wang were identical to those used in the current study, some details of the experimental conditions differed. For example, the number of talkers and vowels used differed (a single talker and three vowels [/i/, /a/, /u/] in Bilger and Wang; 10 talkers and a single vowel /a/ in the current study). However, it has been demonstrated that differences in the vowel accompanying the consonant have little effect

on the patterns of consonant confusions (Gordon-Salant, 1985; Phatak & Allen, 2007).

Grouping of pure-tone audiogram configurations as defined by SINFA-based INDSCAL of CV confusions in quiet revealed different patterns between the study by Bilger and Wang (1976, Figure 5, bottom panels) and the current study (Figure 5, top panels). Bilger and Wang found three distinct subgroups in two-dimensional space. Bilger and Wang's data revealed differences in the average configuration of hearing thresholds that appear clearly discernible (Figure 5, bottom right panel). The NH/gradual group had a slope < 20 dB for 1 kHz ≤ f ≤ 4 kHz. For the same range of frequencies, the flat group had a slope < 5 dB, and the steep group had a slope > 30 dB. For the current study, the slopes of the average hearing thresholds showed great overlap across groups defined by SINFA-based INDSCAL (Figure 5, top right

Figure 5. Audiograms, categorized by INDSCAL. The top panels are audiograms from the current study, defined by the SINFA-based INDSCAL model in quiet. There are 12 and 13 listeners in panels 1 and 2. Middle panels are audiograms from the current study that are grouped by the CM-based INDSCAL model in quiet. There are 15, five, and five listeners in panels A, B, and C, respectively. The bottom panels are pairwise multidimensional scaling-based HI groups for CVs presented in quiet, reported by Bilger and Wang (1976). Eight ears were classified as belonging to the NH/gradual group, six ears as the flat group, and nine ears as the steep group. Average thresholds for all three groups are shown in the panels to the right for purpose of comparison.
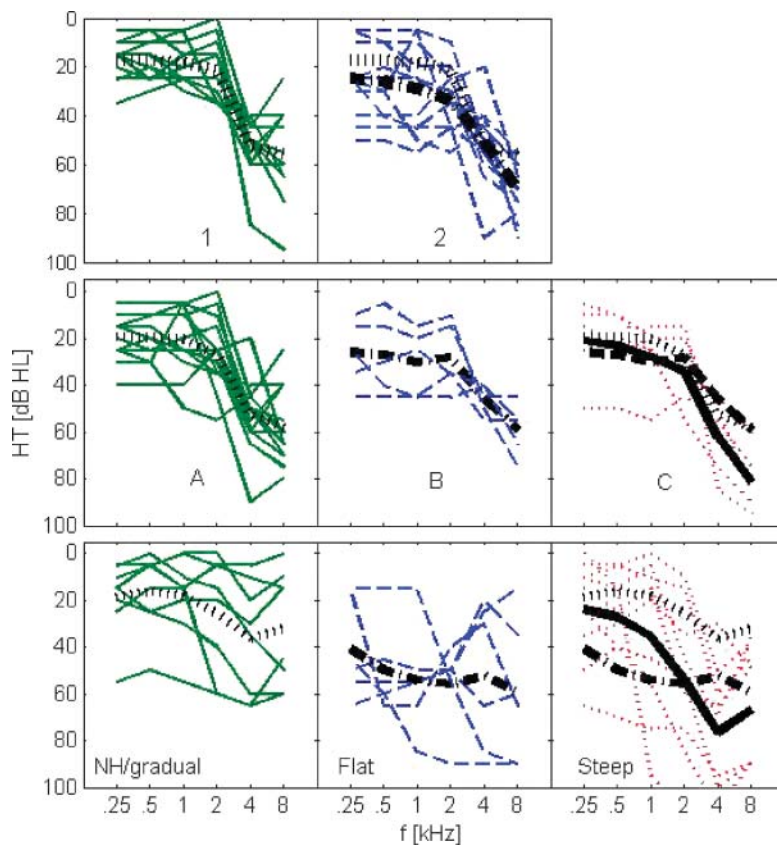
panel). For example, for 0.25 kHz ≤ *f* ≤ 2 kHz, the slopes of group 1 and 2 are somewhat different (<15 dB), but for 2 kHz ≤ *f* ≤ 4 kHz, the slopes of the two groups are similar (<10 dB). Listener grouping, defined by CM-based INDSCAL in the current study (Figure 5, middle panel) was different from that defined by SINFA-based INDSCAL in the current study and in Bilger and Wang. For the current study, the slopes of the average hearing thresholds show great overlap across groups defined by CM-based INDSCAL (Figure 5, middle right panel). Specifically for 1 kHz ≤ *f* ≤ 4 kHz, the slopes of groups A and B are similar (<20 dB), and the slope of group C is < 30 dB.

The cause for the discrepancy in the results defined by SINFA-based INDSCAL between the current study and that of Bilger and Wang (1976) might be talker variation. For the present study, 16 CVs were produced by 10 different talkers, whereas for the Bilger and Wang study, all CVs were produced by a single talker. It has been shown that perceptual confusions are clearly influenced by talker variation (Phatak, Lovitt, & Allen, 2008; Regnier & Allen, 2008). Phatak et al. (2008) showed that different utterances of the same consonant can produce a significant variability in performance scores and confusion patterns. The consonant most often confused with a given target consonant varied depending on the talker. The reason for using multiple talkers in the present study was to measure confusions under more realistic listening conditions. Such conditions may yield results that are more readily generalized but more complex in that the confusions are more distributed even for the same utterance. Thus, it is likely that talker variation is one of the variables that can spread the effect of the audiometric difference across subject space, resulting in inconsistent groupings for performance in quiet as shown in the current study.

The cause for the discrepancy in the results between CM-based INDSCAL in the current study and SINFA-based INDSCAL in the study by Bilger and Wang (1976) appears to result from a difference in input structures for the INDSCAL model. In the study by Bilger and Wang, (dis)similarity matrices for the INDSCAL model were constructed from the indices of feature perception, determined by the SINFA (Wang & Bilger, 1973), whereas for the current study (dis)similarity matrices were normalized, raw CMs. Details of how (dis)similarity matrices for the INDSCAL model were constructed, based on the results of SINFA, appear in the Introduction above. The differences in the structure of (dis)similarity matrices directly alter the iteration process from an arbitrary initial configuration of subject space in the INDSCAL model, resulting in a different estimated configuration of subject spaces (Jones & Young, 1972; MacCallum, 1977; Takane et al., 1977). One of two conclusions made by Wang and Bilger (1973), about identifying distinct

perceptual features for CVs from CMs measured in both in quiet and noise, is that similar information transmission for features does not guarantee similar consonant confusion patterns or vice versa. Thus, it is possible, based on the systematic differences between the present study and that of Bilger and Wang, that the dissimilarity matrices, constructed from information transmission for features (SINFA), are more reflective of audiometric threshold differences than of confusion matrices.

For both Bilger and Wang (1976) and the current studies, audibility might be one of the factors affecting internal structure of perceptual confusions. Bilger and Wang used a presentation level of 40 dB above the subject's SRT, and a MCL (75 dB ~ 85 dB SPL) was used for the current study. Using data given in the study of Bilger and Wang, we computed the average presentation levels for each of the HI groups categorized by SINFA-base analyses as follows: 54.6 dB HL for the NH/gradual group (Figure 5, A panel), 67.6 dB HL for the flat group (Figure 5, B panel), and 67.0 dB HL for the steep group (Figure 5, C panel). For the current study, using the minimum audibility curve (ANSI S3.6-1996), the presentation levels of 75 and 85 dB SPL would be equivalent to 62.5 and 72.4 dB HL. The presentation levels in dB HL for both studies were comparable. However, an inspection of the audiograms given in Figure 5 for both studies indicates that sensation level is too low for some subjects. For example, in the study by Bilger and Wang, three subjects in the NH/gradual group had sensation level less than 10 dB at frequencies >3 kHz; two and four subjects in the flat and steep groups showed the same results. In the current study, six subjects in the A group (Figure 5, middle panel) had sensation level of less than 10 dB at 3 kHz; this result was similarly evident in one and four subjects in the B and C groups, respectively (Figure 5, middle panel). Lower sensation level at high frequencies might affect perception of some consonants such as /sa/ and /ʃa/, but it is unclear how such a lack of audibility affects the confusion patterns. Consequently, it is difficult to predict how listener's groupings observed in both studies will be affected. It would be interesting to see how the relationship between consonant confusions and hearing threshold would be affected if a spectral compensation procedure such as NAL-R is applied to adjust frequency response based on the loudness equalization for each CV.

Another possible influence on the grouping observed in the current study is the characteristics of the noise masker (speech-shaped noise). That is, the presence of a noise stimulus might change the effective hearing loss configuration, making it more similar than different for persons with different losses. If this is the case, then the result of grouping in quiet for the current study should be different from that in noise. This was not the case for

the results of the current study. For example, in Figure 2, seven subjects with flat hearing loss were consistently separated into two groups when syllables were presented in both noise and quiet. Regardless of presence of noise, the two listeners with steeply sloped hearing loss (threshold $\geq$ 30 dB/octave for 1 kHz $\leq f \leq$ 4 kHz) were also consistently classified in the same group. In addition, 3R and 117R in the sloping group were separated from five other subjects in the same group (4L, 4R, 76L, 113R, and 216L) across SNR including the quiet condition. Based on this evidence, it is unlikely that the presence of a noise stimulus changes the effective hearing loss configuration and makes persons with different losses more similar than different. The results of the present study might be useful for hearing aid fitting algorithm research.

For most current hearing aid fitting algorithms, the pure-tone audiogram is the primary input even though the audiogram does not account for the majority of the variance in performance of speech perception in noise. Our results suggest that patients with similar audiometric configurations may require different hearing aid strategies.

Conclusions

A clear predictive relationship between the Pe (SNR) and HT (f), was not found for syllable recognition either in noise or in quiet. The result of a multiple regression model showed that 39% of total variance of the Pe (SNR) was contributed by the HT (f). The result of SINFA-based INDSCAL analysis revealed consistent grouping of listeners across SNRs, but groupings were not consistent with two configurations of pure-tone thresholds. The CM-based INDSCAL analysis showed no systematic relationship between the consonant confusions and the HT (f) at any SNRs, including the quiet condition. Thus, audiometric threshold does not account for the majority of the variance in performance of nonsense-syllable perception in noise when complete CMs were considered.

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